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A matched-pair comparison of inlay and onlay trochlear designs for patellofemoral arthroplasty: no differences in clinical outcome but less progression of osteoarthritis with inlay designs

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Abstract

Purpose To compare clinical and radiographic results after isolated patellofemoral arthroplasty (PFA) using either a second-generation inlay or onlay trochlear design. The hypothesis was that an inlay design will produce better clinical results and less progression of tibiofemoral osteo-arthritis (OA) compared to an onlay design.

Methods Fifteen consecutive patients undergoing isolated PFA with an onlay design trochlear component (JourneyTM PFJ, Smith & Nephew) were matched with 15 patients after isolated PFA with an inlay design trochlear component (HemiCAP[®] Wave, Arthrosurface). Matching criteria were age, gender, body mass index, and follow-up period. An independent observer evaluated patients prospectively, whereas data were compared retrospectively. Clinical outcome was assessed using WOMAC, Lysholm score, and pain VAS. Kellgren–Lawrence grading was used to assess progression of tibiofemoral OA.

Results Conversion to total knee arthroplasty was necessary in one patient within each group, leaving 14 patients

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per group for final evaluation. The mean follow-up was 26 months in the inlay group and 25 months in the onlay group (n.s.). Both groups displayed significant improvements of all clinical scores (p < 0.05). No significant differences were found between the two groups with regard to the clinical outcome and reoperation rate. No significant progression of tibiofemoral OA was observed in the inlay group, whereas 53 % of the onlay group showed progression of medial and/or lateral tibiofemoral OA (p = 0.009).

Conclusion Isolated PFA using either a second-generation inlay or onlay trochlear component significantly improves functional outcome scores and pain. The theoretical advantages of an inlay design did not result in better clinical outcome scores; however, progression of tibiofemoral OA was significantly less common in patients with an inlay trochlear component. This implant design may therefore improve long-term results and survival rates after isolated PFA.

Level of evidence III.

Keywords Patellofemoral arthritis · Patellofemoral arthroplasty · Inlay · Onlay · HemiCAP Wave · Journey PFJ

Introduction

Patellofemoral arthroplasty (PFA) has been used for more than 30 years [6, 37], but is still discussed controversial [27, 31, 35]. Poor clinical outcomes and high failure rates have led to a decline in popularity of PFA in the past [3, 6, 7, 12, 17, 26, 45, 46]. Drawbacks associated with the design of the trochlear component are believed to be the major reason for failures with early implants [31, 32, 35]. Since the introduction of new implant designs, PFA has produced more consistent results and has regained importance in clinical practice [22, 28, 31, 32, 35, 47].

Currently available trochlear components can be divided into two groups: inlay and onlay designs [33-35]. Inlay design trochlear components are implanted flush with the surrounding cartilage after creation of a bone bed within the native trochlea. Onlay design trochlear components completely replace the anterior compartment by using the same anterior cut as known from total knee arthroplasty. Early inlay designs, also considered as first-generation implants, are associated with higher failure rates compared to second-generation onlay designs [3, 7, 26, 35, 43–45]. Therefore, onlay design trochlear components were considered the gold standard for several years [33-35]. However, with the introduction of a second-generation inlay design, which allows for individualized and anatomic trochlear resurfacing, a promising alternative implant became available [10, 14, 22, 42]. Theoretical advantages of more sophisticated inlay designs include less mechanical patellofemoral complications, increased implant stability, unaltered soft tissue tension and extensor mechanism, and less risk for overstuffing of the patellofemoral joint [10, 14, 22, 42]. However, no study so far has compared the outcomes of inlay and onlay design PFA. The purpose of this study was therefore to compare clinical and radiographic results after isolated PFA using either an inlay or onlay trochlear design of second-generation PFA. Based on the theoretical advantages of an inlay design, it was hypothesized that an inlay design will produce better clinical results and less progression of tibiofemoral osteoarthritis (OA) compared to an onlay design.

Materials and methods

Between February 2006 and September 2014, 118 patients were treated with PFA at one single institution (Department of Orthopaedic Sports Medicine, Technical University Munich, Germany). Indications for surgery were disabling noninflammatory patellofemoral OA (grade III-IV according to the Kellgren-Lawrence grading [23]) or chondrosis (grade III-IV according to Outerbridge [41]) refractory to conservative treatment and/or prior surgery [29, 30, 47]. Contraindications were symptomatic tibiofemoral OA with pain during activities of daily living, systematic inflammatory arthropathy, chondrocalcinosis, chronic regional pain syndrome, active infection, and fixed loss of knee motion [30, 47]. Relative contraindications for PFA were uncorrected patellofemoral instability, patellofemoral malalignment, and tibiofemoral malalignment. In those patients, PFA was combined with patellar stabilizing and/or realignment procedures [4, 27, 30, 47], according to an algorithm described in detail elsewhere [22]. For the purpose of this study, only patients who underwent isolated PFA were included (n = 64).

An onlay trochlear design (Journey[™] PFJ, Smith & Nephew, Andover, MA, USA) was the standard implant for several years at our institution. However, with the introduction of a second-generation inlay trochlear design (Hemi-CAP[®] Wave, Arthrosurface, Franklin, MA, USA), the onlay design was subsequently replaced. In total, 15 patients received isolated implantation of the onlay design component between February 2006 and August 2008, and 49 patients received isolated implantation of the inlay design component between September 2008 and September 2014. Since the patients were not randomized preoperatively, a matched-pair analysis was conducted in order to minimize selection bias. Matching criteria were age (± 5 years), gender, body mass index ($\pm 5 \text{ kg/m}^2$), and follow-up period $(\pm 3 \text{ months})$. The patient selection and matching process is shown in Fig. 1.

Implants and surgical technique

The inlay trochlear component used in this series was the HemiCAP[®] Wave Patellofemoral Resurfacing Prosthesis (Fig. 2). This system intends to replicate joint biomechanics by intraoperative joint surface mapping, three-dimensional socket reaming, and implantation of a matching, contoured trochlear inlay component. Eight different implants with varying offsets and radii of curvature are available [22].

Onlay PFA was performed with the JourneyTM PFJ (Fig. 3). This implant intends to restore normal patellar tracking by an asymmetric design with a deepened and lateralized trochlear groove. Four different implant sizes are available for each site [4].

The surgical techniques for both implants have been described in detail elsewhere [4, 22]. We did not routinely resurface the patella. In our clinical practice, the patella is only resurfaced in patients with patellofemoral incongruence because of severe patellar dysplasia, focal osteonecrosis or osteolysis, and subchondral bone defects [24]. In this series, patellofemoral resurfacing was performed in five patients within each group (33 %). Post-operative rehabilitation was identical for both groups. Patients performed partial weight-bearing with 20 kg for 2 weeks, followed by progression of weight-bearing with 20 kg per week. Full range of motion was allowed immediately.

Clinical and radiographic evaluation

An independent observer who was not a participating surgeon followed all patients prospectively. The clinical outcome was evaluated using the WOMAC score [5], Lysholm score [36], and visual analogue scale for pain (pain VAS) [19]. The WOMAC score was assessed according to the

Fig. 1 Flow chart of the patient selection and matching process

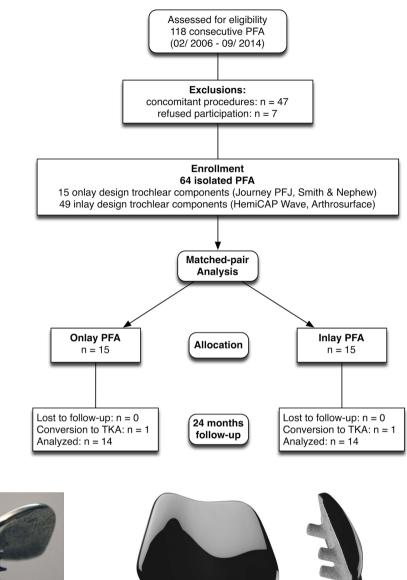




Fig. 2 Second-generation inlay trochlear design (HemiCAP[®] Wave, Arthrosurface, Franklin, MA, USA). Reprinted with kind permission from Arthrosurface

KOOS User's Guide (available at http://www.koos.nu/ KOOSGuide2003.pdf). Standardized answer options were given as five Likert boxes, and each question got a score from 0 to 4. A normalized percentage score (100 indicating no problems and 0 indicating extreme problems) was calculated for each subscale. Radiographic evaluation was performed using the Picture Archiving and Communication System (PACS, Philips Medical Systems, Sectra Imtec AB, Sweden). Radiographs included weight-bearing anteroposterior view, true lateral view, and patellar skyline view.

Fig. 3 Onlay trochlear design (JourneyTM PFJ, Smith & Nephew, Andover, MA, USA). Reprinted with kind permission from Smith & Nephew

The Kellgren–Lawrence grading [23] was used to assess progression of tibiofemoral OA, and the Caton–Deschamps Index [11] was used to assess patellar height. In order to analyse and to compare the preoperative anatomy of the patellofemoral joint, the sulcus angle [9] and congruence angle [38] were measured on axial radiographs, the shape of the patella was graded according to Wiberg [48], and trochlear dysplasia was graded according to Dejour [16].

The study was approved by the institutional review board of the Technical University of Munich (registration number

Table 1 Patient characteristics and matching critical	teria
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	Inlay	Onlay	Significance
Number of patients	15	15	n.s.
Gender distribution [#]			n.s.
Male	73 %	73 %	
Female	27 %	27 %	
Age (years) [#]	48 ± 8	49 ± 8	n.s.
Body mass index (kg/m ²) [#]	27 ± 3	27 ± 3	n.s.
Follow-up (months) [#]	26 ± 11	25 ± 10	n.s.
Surgical history of the ipsilateral k	nee joint		
Patellofemoral ^a	60 %	73 %	n.s.
Others ^b	20 %	7%	n.s.
Trochlear dysplasia (Dejour classification)			n.s.
None	33 %	13 %	
Type A	33 %	80 %	
Type B	7 %	0 %	
Type C	13 %	7%	
Type D	13 %	0 %	
Patellar shape (Wiberg classification)			n.s.
Type I	18 %	50 %	
Type II	73 %	50 %	
Type III	9 %	0 %	
Sulcus angle (°)	137 ± 10	140 ± 6	n.s.
Congruence angle (°)	2 ± 27	9 ± 18	n.s.
Patellar resurfacing	33 %	33 %	n.s.
Reoperations others than TKA ^c	13 %	13 %	n.s.
Conversion to TKA	7 %	7 %	n.s.

Values are given as percentage of the corresponding study group, or as mean $\pm \mbox{ SD}$

n.s. not significant, kg/m^2 kilograms per square metre, *TKA* total knee arthroplasty

Matching criteria

^a Inlay group: Cartilage debridement (n = 6), microfracturing (n = 1), osteochondral autologous transfer (n = 1), open reduction and internal fixation of a patellar fracture (n = 1); Onlay group: Cartilage debridement (n = 7), microfracturing (n = 1), osteochondral autologous transfer (n = 1), open reduction and internal fixation of a patellar fracture (n = 2)

^b Inlay group: Partial resection of the medial meniscus (n = 1), partial resection of the lateral meniscus (n = 1), anterior cruciate ligament reconstruction (n = 1); Onlay group: Partial resection of the medial meniscus (n = 1)

^c Inlay group: Implantation of a new trochlear component because of component disassembly (n = 1), lateral facetectomy of the patella because of lateral hyperpression syndrome (n = 1); Onlay group: Valgus high tibial osteotomy because of medial compartment pain (n = 1), debridement and irrigation because of superficial wound infection (n = 1) 419/13), and all patients gave their written informed consent to participate in this investigation.

Statistical analysis

Data were analysed using SPSS version 22.0 (IBM-SPSS, New York, USA). The nonparametric Wilcoxon test for two related samples was used to compare the pre- and postoperative values within each group. The nonparametric Mann–Whitney U test for independent samples was used to compare patient characteristics, follow-up, clinical scores, and radiographic data between the two groups. All statistical tests were performed two-sided. Statistical significance was considered at p < 0.05. An a priori power analysis was calculated with a difference of 30 points and a SD of 20 points in the Lysholm score. It established a sample size of eight patients per group with $\alpha = 0.05$ and a power of 80 %.

Results

The detailed patient characteristics of both groups are provided in Table 1. Based on the matched-pair design of the study, no significant differences were found between the two groups for gender, age, body mass index, and followup period. In addition, no significant group differences were found for the preoperative anatomy of the patellofemoral joint (sulcus angle, congruence angle, trochlear dysplasia according to Dejour, and patellar shape according to Wiberg), previous knee surgery, number of patients with patellar resurfacing, and reoperations during the study period. One patient within each group was revised to a total knee arthroplasty during the follow-up period and subsequently excluded from the clinical and radiographic evaluation. Therefore, 14 patients in each group were available for final follow-up (Fig. 1).

Clinical results

The detailed results of the clinical scores are shown in Tables 2 and 3. In both groups, statistically significant improvements (p < 0.05) of all analysed scores were observed. In addition, both groups displayed significant improvements of all WOMAC subscales. At final follow-up, no statistically significant difference was found between the two groups for any score. In addition, no significant difference was found when the delta between preoperative and follow-up values was compared between the two groups.

Table 2	Results of th	e Lysholm score	and pain VAS
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	Inlay	Onlay	Significance
Pain VAS			
Preoperative	6 ± 2	8 ± 2	p = 0.016
Follow-up	$4 \pm 3^{\#}$	$4 \pm 3^{\#}$	n.s.
Delta	3 ± 3	4 ± 3	n.s.
Lysholm score			
Preoperative	34 ± 11	32 ± 20	n.s.
Follow-up	$66 \pm 23^{\#}$	$57\pm22^{\#}$	n.s.
Delta	33 ± 25	25 ± 27	n.s.

Values are given as mean \pm SD

Delta describes the difference between preoperative and follow-up values

n.s. not significant, VAS visual analogue scale

[#] Statistically significant improvement compared to preoperative (p < 0.05)

Table 3 Results of the WOMAC score

	Inlay	Onlay	Significance
WOMAC pain			
Preoperative	57 ± 18	48 ± 24	n.s.
Follow-up	$75\pm19^{\#}$	$79\pm22^{\#}$	n.s.
Delta	18 ± 26	31 ± 25	n.s.
WOMAC stiffnes	s		
Preoperative	49 ± 21	56 ± 22	n.s.
Follow-up	$70\pm24^{\#}$	$70\pm17^{\#}$	n.s.
Delta	21 ± 24	14 ± 22	n.s.
WOMAC function	n		
Preoperative	66 ± 14	52 ± 25	n.s.
Follow-up	$80\pm19^{\#}$	$79\pm19^{\#}$	n.s.
Delta	14 ± 21	26 ± 22	n.s.
WOMAC overall			
Preoperative	63 ± 14	51 ± 24	n.s.
Follow-up	$78\pm18^{\#}$	$78\pm19^{\#}$	n.s.
Delta	15 ± 21	26 ± 22	n.s.

Values are given as mean \pm SD

Delta describes the difference between preoperative and follow-up values

n.s. not significant

[#] Statistically significant improvement compared to preoperative (p < 0.05)

Radiographic results

The detailed radiographic results are shown in Table 4. None of the patients in the inlay group showed progression of tibiofemoral OA. In contrast, the onlay group showed significant progression of tibiofemoral OA in the medial (p = 0.008) and lateral (p = 0.046) compartment, with 53 % of the patients showing progression of medial and/or lateral tibiofemoral OA (p = 0.009). Comparing the delta between preoperative and follow-up values of both groups, the onlay group showed a significantly higher delta in the medial compartment compared to the inlay group (p = 0.024). With regard to patellar height, no significant difference between pre- and post-operative was found in the inlay group, whereas a small but statistically significant decrease in patellar height was found in the onlay group (p = 0.022).

Discussion

The main finding of the present study was that isolated PFA using either a second-generation inlay or onlay trochlear design significantly improves functional outcome scores and pain, without significant differences between both implants. However, progression of tibiofemoral OA was significantly more common in patients with an onlay trochlear design.

Outcomes of PFA are mainly influenced by patient selection, surgical technique, and design features of the trochlear component. Early failures of PFA are usually related to patellar maltracking or instability, whereas longterm failures are mainly the result of progressive tibiofemoral OA [8, 13, 33]. Based on the current knowledge, early failures are mainly related to problems associated with the design of the trochlear component [6, 26, 29, 31, 32, 45]. First-generation trochlear components were characterized by an inlay design, which replaced the worn cartilage without addressing the subchondral bone. These implants were associated with poor clinical results and high failure rates [3, 7, 26, 35, 43-45]. Attempts to improve the success rates of PFA have led to the development of secondgeneration trochlear components, which are grossly characterized by an onlay design [35, 44, 47]. These implants are based on the trochlear cuts of total knee arthroplasty, replacing the entire anterior trochlear surface [35]. In general, good short- and medium-term results with low failure rates can be expected with currently available onlay design trochlear components [1, 2, 4, 28, 40]. In a recent review article, Lonner and Bloomfield [33] summarized the results of PFA and concluded that onlay-style trochlear prostheses are associated with lower revision rates and higher functional success rates compared to first-generation inlay-style prostheses. According to Lonner and Bloomfield [33], high success rates and good functional outcomes are more easily achievable with contemporary onlay designs. However, implantation of onlay design components is also associated with specific problems: Since an intramedullary rod guides the anterior femoral cut, malpositioning of the intramedullary guiding in a flexed or extended position increases

the risk of patella catching (Fig. 4a, b). Depending on the thickness of the implant and amount of bone resection, an onlay design may overstuff the patellofemoral joint, leading to increased patellofemoral loads and soft tissue irritation (Fig. 4c) [18, 21, 39]. Furthermore, a too broad component with medial or lateral overhang may cause soft tissue impingement and limited range of motion [32].

Design improvements of PFA not only led to the introduction of onlay design components, but also to the development of improved inlay designs. In the authors' opinion,

Table 4 Radiographic results. Kellgren–Lawrence grading is given as median (interquartile range); progression of tibiofemoral OA is given as number of patients (percentage of the corresponding study group); Caton–Deschamps Index is given as mean \pm SD

	Inlay	Onlay	Significance
KL medial			
Preoperative	2 (1–2)	2 (1-2)	n.s.
Follow-up	2 (1–2)	2 (2-3)#	n.s.
Delta	0 (0–0)	1 (0–1)	p = 0.024
KL lateral			
Preoperative	2 (1–2)	1 (1–2)	n.s.
Follow-up	2 (1–2)	2 (1-2)#	n.s.
Delta	0 (0–0)	0 (0–1)	n.s.
Progression of tibiofemo	oral OA		
Medial	0 (0 %)	7 (47 %)	p = 0.024
Lateral	0 (0 %)	4 (27 %)	n.s.
Medial and/or lateral	0 (0 %)	8 (53 %)	p = 0.009
CDI			
Preoperative	0.9 ± 0.2	1.0 ± 0.1	n.s.
Follow-up	0.9 ± 0.2	$0.9\pm0.2^{\#}$	n.s.
Delta	0.0 ± 0.1	-0.1 ± 0.1	n.s.

Delta describes the difference between preoperative and follow-up values

KL Kellgren-Lawrence, CDI Caton-Deschamps Index, n.s. not significant

[#] Statistically significant difference compared to preoperative (p < 0.05)

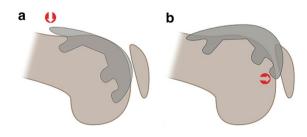
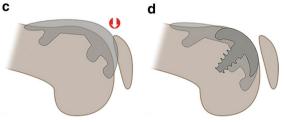


Fig. 4 Problems associated with onlay design trochlear components for patellofemoral arthroplasty. \mathbf{a} A flexed intramedullary guidance increases the risk of patella catching from extension to flexion; \mathbf{b} An extended intramedullary guidance increases the risk of patella catch-

these prostheses must also be considered as second-generation implants. One example of second-generation inlay PFA is the HemiCAP[®] Wave prosthesis. This system uses intraoperative joint surface mapping, three-dimensional socket reaming, and implantation of contoured inlay components in order to more closely reproduce the geometry of the distal femur. Different trochlear components with varying offsets allow for individualized and anatomic trochlear resurfacing. Potential advantages of an inlay design prosthesis include less removal of bone (Fig. 4d), increased intrinsic implant stability, unaltered soft tissue tension and extensor mechanism, and less risk for overstuffing of the patellofemoral joint [10, 14, 42].

The present study is the first that directly compared second-generation inlay and onlay trochlear designs for PFA. Both implants significantly improved functional outcome scores and pain, without significant differences between both groups. In addition, no significant difference between both implants was found with regard to the reoperation rate, which was low in both groups. None of the patients with an inlay component required reoperation because of patellofemoral maltracking or mechanical patellofemoral complications such as catching, snapping, or clunking. We therefore conclude that the development of the secondgeneration inlay component used in the present study has resolved design-specific complications of first-generation inlay designs and can be considered a valuable alternative to currently used onlay designs, with the theoretical advantages of an inlay design component.

Progression of tibiofemoral OA is the most common reason for the failure of PFA using modern prosthetic designs [13, 25, 44]. An interesting finding of the present study was that none of the patients with an inlay component showed progression of tibiofemoral OA, whereas more than half of the patients in the onlay group demonstrated progression of medial and/or lateral tibiofemoral OA. The true reason for this observation remains unknown; however, one hypoth-esis is that the more anatomic approach of the inlay design better reproduces the complex kinematics of the patel-lofemoral joint. Soft tissue irritation due to overstuffing



ing from flexion to extension, and the risk of anterior notching; **c** Risk of anterior overstuffing; **d** Increased bone loss after onlay in comparison with inlay design components

of the patellofemoral joint with an onlay component may cause persistent synovitis, which is a well-known risk factor for the development and progression of OA due to secretion of pro-inflammatory cytokines [15]. Whether an inlay design component also prevents progression of tibiofemoral OA over a longer follow-up period remains unknown.

A specific pitfall of inlay design components is that rotation of the prosthesis is determined by the rotation of the distal femur. In patients with significant internal rotation, isolated inlay PFA may result in patellar maltracking and instability because of an internally rotated trochlear component. In our clinical practice, we therefore combine inlay PFA with a supracondylar femoral derotation osteotomy if femoral antetorsion exceeds 20° [20, 22]. On the other hand, when using an onlay design prosthesis, rotation of the trochlear component is determined by the surgeon, and internal rotation of the distal femur can be corrected to some degree by placing the femoral component in external rotation. An onlay design component might therefore be beneficial in patients with minor rotational malalignment to avoid femoral osteotomy. In addition, an onlay design component might be considered in patients with high-grade trochlear dysplasia, since positioning of an inlay prosthesis can be difficult in such cases, especially for inexperienced surgeons. However, we also use inlay PFA in patients with type C and D dysplasia, and did not observe specific complications so far.

This study has several limitations. First, only a small number of patients were investigated. Despite a relatively large number of PFA performed at our institution, only a small group of patients fulfilled the inclusion criteria. In our clinical practice, PFA is performed with concomitant realignment or stabilizing procedures in about half of the cases. Since the purpose of this study was to compare different trochlear components, only patients with isolated PFA were included. Second, the follow-up is relatively short, and therefore, the long-term outcomes of both prostheses remain unknown. However, since implant-related failures are commonly observed in the early post-operative phase, we believe that the follow-up period was adequate to compare different implants. Third, patients were not randomized preoperatively, and therefore, this study does not provide the highest level of evidence. Nevertheless, a matched-pair design was chosen to achieve adequate comparability by minimizing confounding factors.

With regard to the clinical relevance of the present study, our results suggest that good functional outcome can be achieved with both implant designs. However, given the lower progression of tibiofemoral OA seen in patients with an inlay trochlear component, this implant design may improve long-term results and survival rates after isolated PFA.

Conclusion

Isolated PFA using either a second-generation inlay or onlay trochlear design significantly improves functional outcome scores and pain. The theoretical advantages of an inlay design did not result in better clinical outcome scores compared to an onlay design. However, progression of tibiofemoral OA was significantly less common in patients with an inlay trochlear component.

Compliance with ethical standards

Conflict of interest A. B. Imhoff and P. B. Schöttle are consultants for Arthrosurface. The company had no influence on study design, data collection, and interpretation of the results or the final manuscript.

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